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Original Research

Preparation, Characterization and *In Vitro* Drug Release Studies of 6-mercaptopurine Thin Film

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Abstract	Article Information
Oral thin films of 6-mercaptopurine were fabricated from mucoadhesive polymer, chitosan and polyvinylpyrrolidone for the purpose of prolonging drug release and improving its bioavailability. All fabricated film formulations prepared were smooth and translucent, with good flexibility. The weight and thickness of all the formulations were found to be uniform. These films were also evaluated for surface pH, folding endurance, swelling percentage (% S) and <i>in vitro</i> disintegration time. Scanning Electron Microscopy (SEM) and Fourier Transform Infrared (FTIR) were used to evaluate the physico-chemical nature of the films. <i>In-vitro</i> drug release have shown enhanced release profiles for thin films compared to pure drug and the subave patterne have been found to be and dependent. The release the study	Article History: Received : 20-02-2014 Revised : 25-06-2014 Accepted : 28-06-2014 Keywords: 6-mercaptopurine In Vitro Drug Release SEM FTIR *Corresponding Author:
release patterns have been found to be pH dependant. The results of the study reveals that fabrication of 6-MP oral thin film by using solvent cast technology is a simple and an efficient method for drug delivery to achieve desired therapeutic compliance.	*Corresponding Author: Prem Kumar G
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INTRODUCTION

The thiopurines, azathioprine, 6-mercaptopurine and 6-thioguanine are effective immune-suppressants and anti-cancer agents and are prescribed increasingly to treat inflammatory diseases (Estlin, 2001). 6-mercaptopurine (6-MP) was approved as an antitumor drug by Food and Drug Ádministration (FDA) in 1953 (Cuin et al., 2011) and has been widely used in the treatment of Acute Lymphoblastic Leukemia and Acute Myelocytic Leukemia (Sun et al., 2013; Karim et al., 2013) and other diseases such as rheumatologic disorders, prevention of rejection followina organ transplantation, systemic lupus erythematosus, non-Hodgkin-lymphoma, inflammatory diseases (Crohn's Syndrome and Ulcerative Colitis) and so on (Podsiadlo et al., 2008; Kevadiya et al., 2013).

6-MP is first metabolized to an active form methylated acid (MeTIMP) hypoxanthine thioinosinic by phosphoribosyltransferase (HPRT) within cell to inhibit de novo purine synthesis (Panetta et al., 2006) and later converted to thioguanine, which is a DNA intercalating agent. However, 6-MP undergoes extensive first pass catabolism by XO (Xanthine oxidase) and TPMT methyl transferase) (thiopurine S limiting their bioavailability. So this could lead to a lower bioavailability (about 16%) (Cheok and Evans, 2006), short plasma halflife (0.5-1.5 h) (Zacchigna et al., 2007), with moderate

plasma protein binding (19% to 30%) (Mawatari *et al.*, 2001) and plummeting chemotherapeutic effect. With a view to optimize the therapeutic effect of 6-MP, the objective of this investigation was to formulate mucoadhesive buccal films using chitosan-Polyvinyl pyrolidone (PVP) polymer complex for sustained release of the drug and to evaluate their physico-chemical characteristics by using SEM and FTIR.

MATERIALS AND METHODS

Materials

6-mercaptopurine monohydrate (Assay purity \geq 98.0%), Polyvinyl Pyrrolidine (PVP) (Mw= 13,00, 000), Chitosan low molecular weight (deacetylation \geq 75.0%), Acetic acid glacial (\geq 99.85%) and dialysis tubing cellulose membrane were purchased from Sigma-Aldrich Chemical Co. Ltd. Monobasic sodium phosphate (NaH₂PO₄) and Dibasic sodium phosphate (Na₂HPO₄) were purchased from Emplura[®], Merck Specialities Pvt. Ltd., Bangalore, India.

Preparation of Chitosan-PVP oral thin films

Chitosan solution (2% w/v), was prepared by dissolving chitosan in 1% w/v acetic acid and then 6-mercaptopurine (0.5% w/v) was dispersed in the solution under constant magnetic stirring. PVP solution (2% w/v), was prepared by dissolving PVP in ethanol by stirring it

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continuously for about 10 mnt to obtain clear homogeneous solution. Chitosan-PVP blends solutions (1:2) were prepared by stirring for about half an hour. The obtained homogenous solutions were poured into a plastic mould, covered and kept overnight at room temperature for solvent evaporation. The resulting films were used for further physico-chemical analysis.

Chitosan-PVP Oral Thin Film Characterization Scanning Electron Microscopy (SEM)

The surface morphology of the oral thin films containing drug and polymer were characterized by Field Emission Scanning Electron Microscope (FESEM, FEI Sirion) at operating voltage of 5–30 KV. All images were recorded at working distance of 8-10 mm.

FTIR Analysis

The procedure involving sample preparation and spectral recordings was carried out by previously described method (Stuart *et al.*, 2004). IR spectra of 6-MP, PVP and oral films were recorded using FTIR Nicolet 6700 (Thermo Fisher Scientific, Madisson, WI, USA) operated by Omnic software 8.1. In particular, for oral thin films measurement the spectra were obtained by attenuated total reflectance (ATR) method using smart orbit diamond ATR. Briefly, the formulations were placed individually on the sample plate of the smart orbit and screwed lightly to record IR spectra in ATR mode.

Surface pH

The surface pH of 6-mercaptopurine oral thin films was evaluated by using combined pH electrode. Films were moistened with milli-Q- water and pH was measured at the interphase of water and film (Prem *et al.*, 2014).

Thickness

Thicknesses of these films were measured by calibrated digital Vernier callipers (Mitutoyo 550-203-10, Mitutoyo, Japan). Thickness was measured at four different points in the films and mean value was expressed (Raju *et al.*, 2011).

Folding Endurance

Folding endurance was determined by repeatedly folding the film (4 X 4 cm) at the same point until a breaking point was achieved. Number of times the film could be folded at the same point without breaking was considered as folding endurance value. All the tests were performed four times and mean of the values was reported (Mona *et al.*, 2012).

Swelling Percentage (% S)

Swelling index for the films was estimated in simulated salivary fluid at pH 6.8. Briefly, films (surface area 4 cm²) were weighed and transferred onto a petriplate containing buffer media (Wang *et al.*, 2000). At definite time interval (15s), films were removed, blotted quickly with adsorbent paper, and then weighed. The percentage of water uptake was calculated as follows where W_f is the weight of wet grafted films and W_i is the weight of dry grafted films.

% S =
$$\frac{(W_f - W_i)}{W_i}$$
 x 100

In Vitro Disintegration Time

In vitro disintegration time was measured by following monograph from United States Pharmacopeia (USP) using disintegration test apparatus (LABINDIA, DS8000) (United States Pharmacopoeia, 2009).

Drug Content

A sample of 3 cm² was dissolved in 10 ml methanol by vortex for 5 minute to extract drug from film and filtered through whatman filter paper and analyzed spectrophotometrically at 325 nm using methanol as a blank (Senthil *et al.*, 2010).

In Vitro Drug Release

In vitro drug release studies were performed using USP Apparatus-I at 50 rpm and 600 ml of PBS (pH 3.4, 6.4 and 7.4) at 37±0.5°C. A calculated 10 mg (conc. 2mg/ml) of pure drug and Chitosan-PVP thin film were separately placed in dialysis tube and immersed in PBS at above mentioned pH. At predetermined time intervals (0, 15, 30 min, 1 h, 2 h, 3 h, 4 h, 8 h, 12 h, 16 h, 24 h and 48 h, an aliquot of 4 ml of the release media was withdrawn and the concentration of the drug in release media was estimated by UV spectroscopy (Evolution 300; Thermo Fisher Scientific, USA) at 325nm. The dissolution medium was replaced with fresh buffer (4ml) to maintain constant total volume (Manohara *et al.*, 2014).

RESULTS AND DISCUSSION Physico-chemical Characterization

SEM Analysis

The prepared oral thin film of 6-MP is depicted in Figure 1. Scanning electron micrographs of the 6-MP thin film with low and high magnification images are depicted in the Figure 2a and 2b respectively. The diameter (500nm- 2μ m) of the distributed 6-MP microparticles in the film has been confirmed (Image software, provided by National Institutes of Health, USA).



Figure 1: 6-MP oral thin film prepared by PVP-chitosan polymer complex

FTIR Analysis

IR spectra of 6-MP and Chitosan-PVP showed the prominent peaks for functional group like N-H, C-H (aliphatic and aromatic), C-O and S-H. Fundamental vibrations of primary functional groups and its frequency (cm⁻¹) of 6-MP, PVP-chitosan and 6-MP loaded PVP-Chitosan thin films are depicted in Figure 3a, 3b, and 3c. Rresults suggests that on comparing the 6-mp films with PVP-Chitosan films,there is no interaction between the 6-mp and PVP-Chitosan polymer complex which is confirmed by the preence of prominent peaks of functional groups and absence of any additional functional groups. (Figure 3 and Table 1).

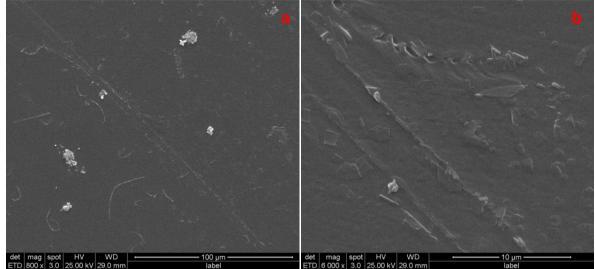


Figure 2: SEM images of PVP-Chitosan oral thin film of 6-mercaptopurine with low (a) and high (b) magnification

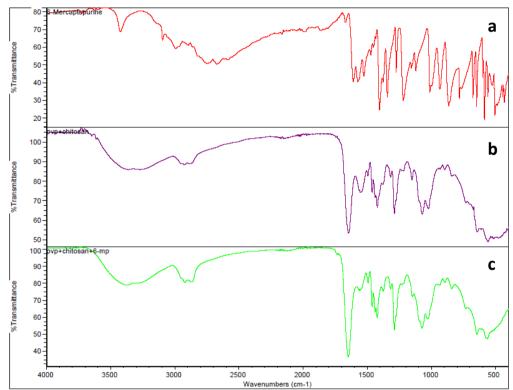


Figure 3: IR spectra of a) 6-mercaptopurine, b) PVP-Chitosan and c) 6-Mercaptopurine loaded PVP-Chitosan thin film

Table1: IR spectroscopic fundamental vibrations and frequencies (cm⁻¹) of 6-MP, PVP-Chitosan and 6-MP thin film

6-MP		PVP-Chitosan		6-MP thin film	
Fundamental Vibrations	Frequency (cm⁻¹)	Fundamental Vibrations	Frequency (cm ⁻¹)	Fundamental Vibrations	Frequency (cm⁻¹)
N-H (stretch)	3424.27	N-H (stretch)	3352.38	N-H (stretch)	3419.28
N-H (Bend)	1527.17	N-H (Bend)	1590.59	N-H (Bend)	1568.79
C-H(stretch)	3095.11, 2994.48	C-H(stretch)	2871.53	C-H(stretch)	3095.13, 2994.04
C-N	1343.98	C-N	1024.39	C-N	1343.91
C=N	1609.31	O-H	3200	C-O	1011.73
C=C	1669.70	C-O	1377.28	S-H	2672.36
S-H	2672.65				

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Surface pH

The surface pH of oral films has been determined in order to investigate the effect of pH on oral mucosa (Prem Kumar *et al.*, 2014). The determined surface pH of the 6-MP film was in range of 6.7 ± 0.1 , which was almost neutral and irritation free to the mucosal lining of the oral cavity.

Thickness

The films were evaluated for thickness using digital Vernier calipers and mean value was found to be 0.436±0.003 mm which indicates the uniformity of the film (Raju *et al.*, 2011).

Folding Endurance

Folding endurance helps in determining the mechanical strength of the films. Higher the folding endurance higher is the mechanical strength (Semalty *et al.*, 2008). The folding endurance of the drug loaded films was 560 which signifies that these films are strong enough to handle.

Swelling Percentage (S%)

Penetration of solvent into the polymer matrix leads to increased weight of the films and facilitates diffusion of drug molecules from bulk of the matrix to external environment (Brazel and Peppas, 2000). The mean swelling percentage was found to be 30.63%.These results imply that the absorption of water by these films was considerable for the drug release. Indeed higher swelling properties can cause discomfort in oral cavity due to their bulk properties.

In Vitro Disintegration Time

Disintegration time gives an indication about onset of action which is desirable for oral thin films (Mishra and Amin, 2009). The calculated mean time for the film to disintegrate into complete fine particles was 0.36 minute and to completely disappear into the solution was 1.21 minute. These values indicate that these films have optimum disintegration time.

In Vitro Drug Release Studies

In order to investigate 6-MP release behaviour of PVP-Chitosan thin films, the thin films were incubated in different release media (phosphate buffer pH: 3.4, 6.4 and 7.4) and assessed by double beam UV-visible spectrophotometer. Figure 4 demonstrates 6-MP release profiles up to 48h of incubation period. As shown in Figure 4, PVP-Chitosan thin films showed an initial burst release of 6-MP in a period of 4-6 h for all incubation media (Avdin and Pulat, 2012). After this initial burst effect, a slower sustained and controlled release occurred throughout the incubation period. Cumulative drug release profiles of 6-MP thin film at pH 3.4 (62%), 6.4 (72%) and 7.4 (82%); were better than release profiles of pure drug (46%, 48% and 45%) (Fig 4a, 4b and 4c). We could also observe significant fall in concentration of 6-MP pure drug (pH 3.4) from 16 hrs onwards, when compared to 6-MP thin film, whereas at pH 6.4 and 7.4 there was no sudden decline in concentration. Release profiles supported that 6-MP molecules were encapsulated among the positively charged hydrophilic chains.

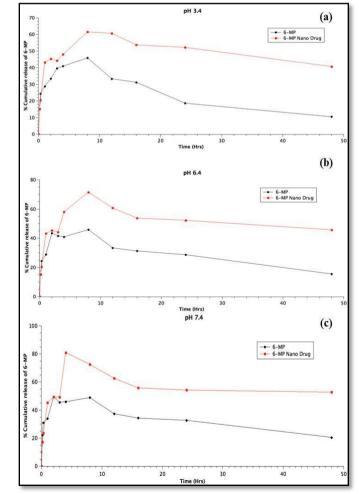


Figure 4: In vitro drug release of 6-MP from PVP-Chitosan thin film at pH a) 3.4 b) 6.4 c) 7.4

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CONCLUSIONS

In this study, we prepared 6-MP loaded PVP-Chitosan thin films for enhanced drug delivery. Results of the SEM images confirmed decreased size of the drug in the film. FTIR spectrum showed non-interaction of 6-MP and PVP-Chitosan polymer matrix. *In vitro* drug release of 6-MP from the thin film has enhanced to a considerable extent. So these formulations can be an alternative for delivering 6-MP, which could enhance solubility, bioavailability with its sustaining drug release process. The preparation of drug loaded PVP-chitosan films is a simple technique that can be easily scaled up.

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