

## Original Research Article

# Formulation, characterization and optimization of nebivolol-loaded sustained release lipospheres

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### Abstract

**Purpose:** To formulate, characterize and optimize nebivolol-loaded sustained release lipospheres (LPs) using beeswax (BW) as the drug carrier.

**Methods:** Nebivolol-loaded LPs were formulated using solvent evaporation technique (SET) and characterized. The impact of independent variables on responses such as percentage yield (PY), entrapment efficiency (EE) and drug release after 12 h (DR12) was assessed using central composite design (CCD). Numerical and graphical optimization techniques were also used to evaluate outcomes of the measured responses.

**Results:** Twenty micron-sized (20 - 100  $\mu$ m), smooth spherical LPs with good rheological properties were produced. The yield ranged from 33 (F10) to 81 % (F6), while EE ranged from 32 (F4 and F9) to 69 % (F6). The results of rheological evaluation revealed angle of repose > 24 o, Hausner's ratio > 1.5, and Carr's index ranging from 13 to 19 %. Fourier-transform infrared (FTIR) spectroscopy, differential scanning calorimetry (DSC) and x-ray diffraction (XRD) revealed nebivolol and BW compatibility, and the absence of possible interactions between formulation components. Duration of nebivolol release was strongly associated with BW concentration and formulation F15 showed minimum drug release (46 %). Drug release was significantly higher in formulations with similar BW concentrations and low Tween-20 (T-20) concentrations (F1 and F11) than in formulations with high T-20 concentrations (F2,  $p < 0.05$ ). The zeta potential of deflocculated LPs ranged from +15 to +35 mV. Nebivolol release (46 - 85 %) at pH 6.8 was significantly affected by BW concentration and it followed zero order model.

**Conclusion:** The results obtained in this study have shown that BW is a suitable material for producing an effective sustained release formulation. The mechanism of drug release in nebivolol- loaded LPs is diffusion accompanied by erosion.

**Keywords:** Lipospheres, Nebivolol, Beeswax, Formulation, Central composite design

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## INTRODUCTION

Hypertension, congestive heart failure (CHF), myocardial infarction (MI), cerebral diseases and

nephropathy result in the death of millions of people globally [1]. At present, the treatment strategies for cardiovascular diseases (CVDs) only serve as mere palliatives [2]. There is increasing demand for sustained delivery

systems that can promote heart function [3,4]. For this purpose, novel formulations such as LSs provide great advantages. Lipospheres are sustained release formulations employed in disease conditions requiring plasma drug concentration that can be sustained for a prolonged period, and they are used for convenient delivery of semi-synthetic, synthetic and biological agents [5]. They can hold both hydrophobic and hydrophilic drugs, and they are physically stable and economically viable. In addition, LSs reduce dose frequency and side effects, and enhance patient compliance [6]. They are formulated from solid lipids characterized by low melting points (65 °C), good biocompatibility and biodegradability, absence of toxicity and ease of production [7]. As a drug carrier, BW can sustain drug release and enhance its bioavailability [7,8].

Nebivolol, a drug used as first-line treatment for hypertension, is a selective beta-blocker which induces vasodilatation via the generation of nitric oxide (NO) [4]. Although nebivolol is highly effective and more generally accepted than other antihypertensive agents, it requires frequent dosing because of its poor solubility, bioavailability (< 40 %) and short plasma half-life (2 h) [9, 10]. Therefore, BW is usually used to improve its solubility and bioavailability. The aim of this study was to formulate, characterize and optimize nebivolol-loaded sustained release LS using BW as drug carrier.

## EXPERIMENTAL

### Materials

Nebivolol was a product of Nabi-Qasim Pharmaceuticals (Pvt) Ltd. (Pakistan). Potassium dihydrogen phosphate (KH<sub>2</sub>PO<sub>4</sub>) and Tween-20 (T-20) were purchased from Merck (Germany). Infra-red grade cellulose dialysis tube and BW were obtained from Sigma Aldrich (USA), while potassium bromide (KBr) was a product of Fischer Scientific (UK). Equipment used included X-ray diffractometer (Bruker AXS, USA) and Zetasizer (Malvern Instruments Ltd., UK).

### Preparation of LS

Nebivolol-loaded LS were prepared using SET. Nebivolol and BW were dissolved in 50 ml chloroform and the resultant solution was added to T-20 preheated at 75 °C and then homogenized to obtain a pre-emulsion [12]. The pre-emulsion was mixed with cold water and stirred using a magnetic stirrer. The LS formed were recrystallized at room temperature and

filtered using 0.45 µm filter paper, and dried using a desiccator. The procedure was performed in triplicates with the aqueous phase and nebivolol concentration kept constant.

### Central composite design

The CCD was performed using Design Expert (8.0.6.1) [11]. The different LS formulations were designed with concentrations of BW and T-20, and stirring speed (SS) as independent variables, while PY (Y<sub>1</sub>), EE (Y<sub>2</sub>) and DR<sub>12</sub> (Y<sub>3</sub>) were the dependent variables/responses. The compatibility of nebivolol and BW was evaluated using FTIR spectroscopy, DSC and XRD. The particle sizes, rheologies, morphologies and zeta potential of the formulated LS were also determined. Release profiles of the LS were evaluated using kinetic models such as zero order, first order, Higuchi and Korsmeyer Peppas. Numerical and graphical optimization techniques were used to create conditions for producing optimum intensity of the measured responses.

### Rheological studies

Rheological evaluation was carried out on the formulated LS based on the method described by Reithmeier *et al* [13] and Carr's index, Hausner's ratio, and angle of repose were determined (Table 1).

**Table 1:** Rheological parameters of formulated LS

Flow parameter	Equation	Range
Carr's index (%)	$I = [(V_b - V_t)/V_t] \times 10$	12 - 19
Hausner's ratio	$HR = \rho_t/\rho_b$	< 1.25
Angle of repose (°)	$\tan\theta = h/r$	< 30

### Determination of PY

The final constant weight (W) of dried LS was divided by the total weight (TW) of all solid lipids used in LS formulation to obtain the yield (Y) of lipospheres as in Eq 1 [14].

$$Y = W/TW \dots\dots\dots (1)$$

### Evaluation of EE

Portions of LS were crushed and dispersed in phosphate buffer (pH 7.4) for 24 h. After dilution, absorbance was read at 282 nm using UV-visible spectrophotometer, and the EE was calculated as in Eq 2 [10,14].

$$EE = ADA/TDA \times 100 \dots\dots\dots (2)$$

where ADA is the actual concentration of neбиволол, and TDA is the theoretical concentration of neбиволол.

### Evaluation of drug release *in vitro*

This lasted 12 h and was performed using Drug Dissolution Apparatus II USP (Paddle) immersed in phosphate buffer, pH 6.8, and maintained at  $37 \pm 0.5$  °C. The LS was put in a dialysis tube containing 5 ml of dissolution medium, and immersed in dissolution vessel containing 900 ml of dissolution medium. After a specified time interval, an aliquot (5 ml) was withdrawn and equal volume of freshly prepared medium was added to the vessel. After further dilution of the sample, absorbance was read at 282 nm [15].

### Drug release kinetics

The drug release data were analyzed using kinetic models such as zero order, first order, Korsmeyer Peppas, Hixson-Crowell and Higuchi's. The mathematical equations used are shown in Eqs 3 – 7.

$$F_t = K_0 t \dots\dots\dots (3)$$

$$\log F = \log F_0 - \frac{K_t}{2.303} \dots\dots\dots (4)$$

$$F = K_H t^{1/2} \dots\dots\dots (5)$$

$$F_0^{1/2} - F_t^{1/2} = K_{HC} \times t \dots\dots\dots (6)$$

$$M_t/M_\infty = K_2 t^n \dots\dots\dots (7)$$

### Analysis of variance (ANOVA) of two-factor interaction (2FI) model

2FI model was analyzed using ANOVA at 5 % significance level. Value of  $p < 0.05$  was taken as an indication that the model was significant for  $Y_1$  and  $Y_2$ .

### FTIR spectroscopy

The FTIR spectra of neбиволол, BW and neбиволол-loaded optimized formulation (OF) were recorded and analyzed using FTIR spectrophotometer. Before analysis, the mixture of LS and KBr was pelleted. Resolution of  $2 \text{ cm}^{-1}$ , hydraulic pressure of  $150 \text{ kg/cm}^2$  and scanning range between 400 and  $4000 \text{ cm}^{-1}$  were used [15].

### Differential scanning calorimetry

Appropriate amounts of neбиволол, BW and OF (2 mg each) were separately heated at the rate of  $10 \text{ }^\circ\text{C/min}$  from 0 to  $220 \text{ }^\circ\text{C}$  in a sealed aluminium pan under nitrogen flow rate of 20 ml/min, and analyzed using a thermal analyzer [15].

### X-ray diffraction

The samples were irradiated with monochromatized X-rays of Cu-K $\alpha$  using D-8 advance X-ray diffractometer at a current of 40 mA, with scanning capacity of  $2 \text{ }^\circ \text{ min}^{-1}$  (diffraction angle- $2\theta$ ) from 0 -  $45^\circ$  [15].

### Scanning electron microscopy (SEM)

Optimized LS were positioned on a double adhesive tape on aluminum stub. Gold coating of stubs was performed under argon atmosphere, and photomicrographs of LS were obtained using scanning electron microscope (x500) at 10 kV [15].

### Zeta potential and particle size measurements

The charges on surfaces of optimized LS were measured by evaluating their electrophoretic mobilities in a U-shaped tube at  $25 \text{ }^\circ\text{C}$  using Malvern Zetasizer [15].

### Statistical analysis

Measurement data are expressed as mean  $\pm$  SD. The statistical analysis and CCD were performed using Design Expert (8.0.6.1) [16]. The optimized formulation was selected on the basis of desirability and numerical optimization functions of Design Expert. Regression analysis was also performed on the measured responses to determine the adequacy and suitability of proposed models. Where appropriate, values of  $p < 0.05$  were considered statistically significant.

## RESULTS

### Formulation components and measured responses

The PY ranged from 33 (F10) to 81 % (F6). Lipospheres with high BW concentrations and low T-20 concentrations formulated at low SS (F4, F9, F10, F11, F13 and F20) had PY  $< 50$  %. Formulations containing the same concentrations of T-20 and BW (F4 and F10) had high PY (44 %), but the PY of F4 was significantly higher than

that of F10 (33 %) ( $p < 0.05$ ). The EE ranged from 32 (F4 and F9) to 69 % (F6).

Although F5 and F6 had the same BW concentrations and were formulated at the same SS, both formulations had different EE (39 and 69 %, respectively). Formulations such as F9, F10 and F11 which had low concentrations of BW and T-20 had minimum EE (Table 2).

### Rheological properties

As shown in Table 3, the rheological properties of LS showed Carr's index ranging from 13 - 19

%, angle of repose  $> 24^\circ$  and Hausner's ratio  $> 1.5$ .

### Optimization of data and model validation

The statistical model selected 2FI for PY and EE, and the suggested relations are shown in Eqs 8 and 9 for  $Y_1$  and  $Y_2$ , respectively.

$$Y_1 = +37.23 - 22.55X_1 - 7.610X_2 + 0.014X_2 + 30.00X_1X_2 - 4.33X_1X_2 - 4.44X_2X_2 \dots\dots\dots (8)$$

**Table 2:** Formulation components and measured responses

Formulation	Formulation component (Coded level)	Formulation component (Actual level, % w/v)			Response (%)		
		BW	T-20	SS	$Y_1$ (PY)	$Y_2$ (EE)	$Y_3$ (DR <sub>12</sub> )
F1	Factorial (-1, -1, +1)	0.75	0.50	3000	58.00 ± 2.71	44.00 ± 1.33	72.00 ± 3.13
F2	Factorial (-1, +1, +1)	0.75	1.25	3000	67.00 ± 2.89	52.00 ± 1.76	56.00 ± 3.36
F3	Center (0, 0, 0)	1.25	0.88	2250	51.00 ± 2.54	39.00 ± 1.82	61.00 ± 3.53
F4	Factorial (+1, -1,+1)	1.75	0.50	3000	44.00 ± 2.98	33.00 ± 2.33	72.00 ± 3.19
F5	Center (0, 0, 0)	1.25	0.88	2250	50.00 ± 2.74	39.00 ± 2.03	59.00 ± 3.87
F6	Axial (0, +β, 0)	1.25	1.51	2250	81.00 ± 2.88	69.00 ± 1.89	50.00 ± 3.45
F7	Center (0, 0, 0)	1.25	0.88	2250	50.00 ± 3.15	39.00 ± 2.24	60.00 ± 3.98
F8	Center (0, 0, 0)	1.25	0.88	2250	50.00 ± 2.97	39.00 ± 2.45	60.00 ± 4.23
F9	Axial (0, -β, 0)	1.25	0.24	2250	40.00 ± 2.47	33.00 ± 2.86	85.00 ± 3.67
F10	Factorial (+1, -1, -1)	1.75	0.50	1500	33.00 ± 2.82	31.00 ± 1.91	76.00 ± 2.73
F11	Factorial (-1, -1, -1)	0.75	0.50	1500	42.00 ± 2.56	33.00 ± 2.34	80.00 ± 2.51
F12	Factorial (-1, +1, -1)	0.75	1.25	1500	50.00 ± 3.11	42.00 ± 1.95	70.00 ± 3.71
F13	Axial (+β, 0, 0)	2.09	0.88	2250	44.00 ± 3.31	35.00 ± 2.37	49.00 ± 4.23
F14	Axial (-β, 0, 0)	0.41	0.88	2250	68.00 ± 2.31	55.00 ± 2.18	52.00 ± 3.22
F15	Factorial (+1, +1, +1)	1.75	1.25	3000	74.00 ± 2.67	61.00 ± 2.07	46.00 ± 3.11
F16	Axial (0, 0, +β)	1.25	0.88	3511	64.00 ± 2.78	55.00 ± 2.24	55.00 ± 3.77
F17	Factorial (+1, +1, -1)	1.75	1.25	1500	65.00 ± 2.42	54.00 ± 1.66	56.00 ± 3.34
F18	Center (0, 0, 0)	1.25	0.88	2250	50.00 ± 3.81	39.00 ± 1.51	60.00 ± 4.03
F19	Center (0, 0, 0)	1.25	0.88	2250	50.00 ± 3.63	39.00 ± 2.23	60.00 ± 3.44
F20	Axial (0, 0, -β)	1.25	0.88	988.6	45.00 ± 2.57	37.00 ± 2.43	76.00 ± 3.78

**Table 3:** Rheological properties of LS

Formulation	Angle of repose (°)	Hausner's ratio	Carr's index (%)
F1	18.00 ± 1.25	1.10 ± 1.88	16.00 ± 1.37
F2	16.00 ± 1.66	1.02 ± 1.66	13.00 ± 1.86
F3	20.00 ± 1.82	1.13 ± 0.89	18.00 ± 0.77
F4	19.00 ± 0.96	1.11 ± 1.77	16.00 ± 0.97
F5	19.00 ± 1.23	1.14 ± 0.98	19.00 ± 1.09
F6	17.00 ± 1.89	1.03 ± 0.96	14.00 ± 1.67
F7	18.00 ± 1.24	1.10 ± 1.65	15.00 ± 0.96
F8	20.00 ± 2.26	1.12 ± 1.83	17.00 ± 0.94
F9	16.00 ± 1.09	1.03 ± 0.89	13.00 ± 1.76
F10	23.00 ± 1.04	1.20 ± 1.61	19.00 ± 1.70
F11	20.00 ± 1.98	1.21 ± 1.67	17.00 ± 1.83
F12	16.00 ± 0.95	1.01 ± 2.33	13.00 ± 1.86
F13	20.00 ± 1.79	1.12 ± 2.66	18.00 ± 1.75
F14	16.00 ± 1.56	1.09 ± 1.92	14.00 ± 0.91
F15	17.00 ± 1.85	1.08 ± 1.93	15.00 ± 0.88
F16	22.00 ± 1.78	1.11 ± 2.07	19.00 ± 0.93
F17	20.00 ± 1.46	1.12 ± 2.03	18.00 ± 1.88
F18	18.00 ± 1.95	1.10 ± 1.35	15.00 ± 0.92
F19	16.00 ± 1.34	1.07 ± 1.77	13.00 ± 1.72
F20	20.00 ± 1.89	1.12 ± 0.97	18.00 ± 1.37

$$Y_2 = +9.808 + 10.75X_1 - 26.39X_2 + 1.73X_2 + 26.00X_1X_2 - 0.013X_1X_2 - 5.77X_2X_2 \dots \dots \dots (9)$$

Drug release ( $Y_3$ ) followed the quadratic model and suggested Eq 10 for  $Y_3$ .

$$Y_3 = +118.08 - 24.347X_1 - 42.62X_2 + 0.02X_3 - 13.75X_1X_2 + 2.65X_1X_3 - 5.30X_2X_3 - 9.41X_1^2 + 26.07X_2^2 + 5.27X_3^2 \dots \dots \dots (10)$$

The maximum to minimum ratio for measured responses ( $Y_1 = 2.45$ ,  $Y_2 = 2.07$  and  $Y_3 = 1.85$ ) was < 3.

**Regression analysis for the measured responses**

Predicted  $R^2$  for the measured responses were very close to their adjusted  $R^2$ , and signal to noise ratio measured from adequate precision was > 4 (Table 4).

**Table 4:** Outcomes of regression analysis for the measured responses

Parameter	$Y_1$	$Y_2$	$Y_3$
R-Squared	0.8756	0.8488	0.9509
Adjusted R-Squared	0.8182	0.7790	0.9067
Predicted R-Squared	0.6285	0.8715	0.7899
Adequate precision	13.637	11.534	17.803
Mean	53.85±5.26	57.25±5.74	62.75±3.37
CV (%)	9.77	10.04	5.37
PRESS	1073.81	1721.35	847.04

**Three-dimensional (3D) surface graphs**

The 3D graphs showing interaction effect of two factors, while keeping the third factor constant are shown in Figure 1.

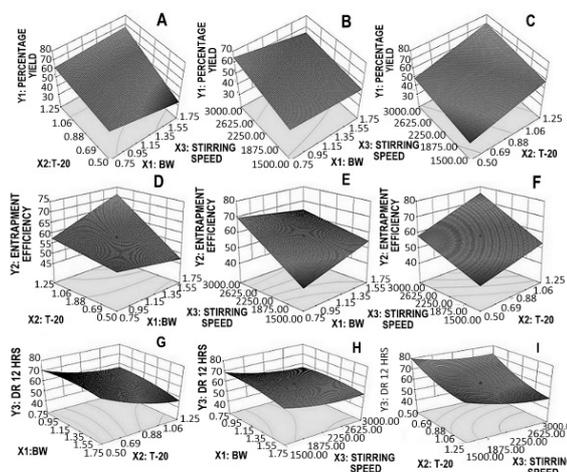
**In vitro drug release profiles of the formulations**

Nebivolol release time was strongly associated with BW concentration and F15 showed minimum drug release (46 %). Drug release was significantly higher in formulations with similar BW concentration and low T-20 concentration (F1 and F11) than in formulations with high T-20 concentration (F2) ( $p < 0.05$ ; Figure 2).

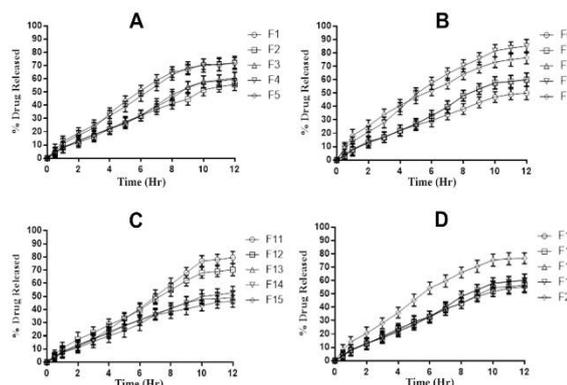
**Outcomes of ANOVA of the measured responses**

The results of ANOVA showed that the applied models were significant ( $p < 0.0001$ ), and values

of  $f$  for  $Y_1$ ,  $Y_2$  and  $Y_3$  were 15.25, 12.16 and 21.25, respectively. The results also showed  $prob > f$  (Table 5).



**Figure 1:** Three-dimensional (3D) response surface plots. **A:** effect of  $X_1$  and  $X_2$  on  $Y_1$ ; **B:** effect of  $X_1$  and  $X_3$  on  $Y_1$ ; **C:** effect of  $X_2$  and  $X_3$  on  $Y_1$ ; **D:** effect of  $X_1$  and  $X_2$  on  $Y_2$ ; **E:** effect of  $X_1$  and  $X_3$  on  $Y_2$ ; **F:** effect of  $X_2$  and  $X_3$  on  $Y_2$ ; **G:** effect of  $X_1$  and  $X_2$  on  $Y_3$ ; **H:** effect of  $X_1$  and  $X_3$  on  $Y_3$ ; **I:** effect of  $X_2$  and  $X_3$  on  $Y_3$



**Figure 2:** In vitro drug release profiles of A (F1 - F5), B (F6 - F10), C (F11 - F15) and D (F16 - F20)

**Optimized formulations**

The OF suggested by optimization techniques was prepared and characterized. The desirability of measured responses was close to 1, and prediction error was at lower level (Table 6). The drug release profiles dominantly followed zero order model since obtained  $R^2$  for zero order was greater when compared with  $R^2$  for the other models (Table 7).

**FTIR spectra and thermal characteristics**

The spectra of nebivolol and BW were compared with FTIR-spectrum of OF. Characteristic aliphatic N - H, alkanes C = C and C - H stretches were observed at  $3185 \text{ cm}^{-1}$ ,  $2319 \text{ cm}^{-1}$

<sup>1</sup> and 1490 cm<sup>-1</sup>, respectively in nebigivolol spectrum and nebigivolol-loaded OF. Carbonyl and sulphur-oxy groups were also visible at 1536 and 1074 cm<sup>-1</sup>, respectively in the FTIR-spectrum of OF (Figure 3). The specific endothermic peaks relevant to melting point of BW and nebigivolol were quite visible at 65 °C (Figure 3 B) and at 221 °C (Figure 3 C), respectively. The peak associated with melting of nebigivolol in OF at 221 °C was also revealed (Figure 3 A).

### X-ray diffraction properties

The x-ray diffractograms revealed the presence of characteristic peaks of nebigivolol at 2θ of 25°, 30° and 40° without any impact on diffraction positions (Figure 4B). The LS of optimized formulations were spherical in shape (Figure 5).

**Table 5:** Analysis of variance showing the effect of factors on responses

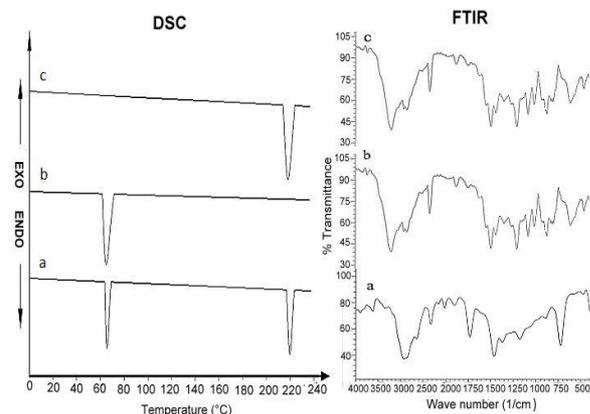
Source	PY (Y <sub>1</sub> )		EE (Y <sub>2</sub> )		DR <sub>12</sub> (Y <sub>3</sub> )	
	f	p prob > f	f	p prob > f	f	p prob > f
Model	15.25	< 0.0001	12.16	< 0.0001	21.25	< 0.0001
BW	4.53	0.0013	1.87	0.01946	7.06	0.0021
T-20	57.95	< 0.0001	21.25	0.0005	110.38	< 0.0001
SS	19.11	0.0008	37.70	< 0.0001	32.78	0.0002
X <sub>1</sub> X <sub>2</sub>	9.15	0.0098	5.76	0.0021	4.40	0.0032
X <sub>1</sub> X <sub>3</sub>	0.76	0.3980	5.76	0.0321	0.70	0.0042
X <sub>2</sub> X <sub>3</sub>	4.519	0.9474	0.64	0.0438	1.58	0.0066
X <sub>1</sub> <sup>2</sup>					7.03	0.0243
X <sub>2</sub> <sup>2</sup>					16.96	0.0021
X <sub>3</sub> <sup>2</sup>					11.04	0.0077
LOF	167.92	0.0006	79.89	0.0008	55.80	0.0002

**Table 6:** Composition of OF

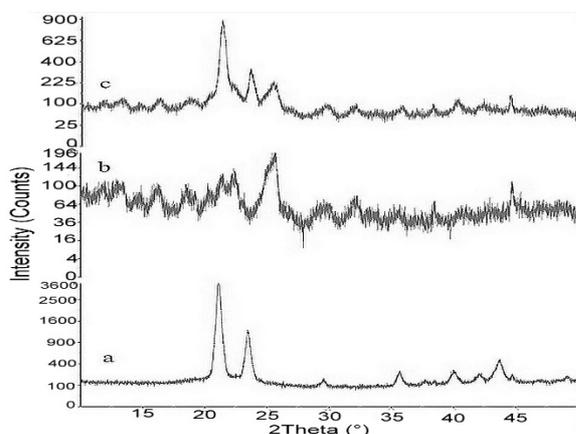
Independent variable	Optimum level	Dependent variable/response	Predicted value	Observed value	Prediction error	Desirability level
X <sub>1</sub>	1.75	Y1	71.75	75.8	1.54	0.891
X <sub>2</sub>	1.25	Y2	77.71	78.8	1.8	
X <sub>3</sub>	3000	Y3	43.83	46.7	1.5	

**Table 7:** Release kinetics of LS formulations

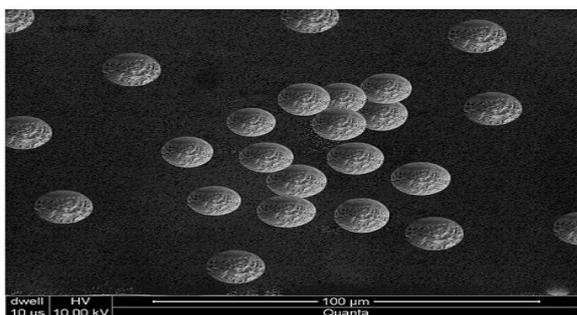
Formulation	Zero order		First order		Higuchi		Hixson-Crowell	Korsmeyer-Peppas		
	R <sup>2</sup>	K <sub>0</sub>	R <sup>2</sup>	K <sub>1</sub>	R <sup>2</sup>	K <sub>H</sub>	R <sup>2</sup>	K <sub>HC</sub>	R <sup>2</sup>	N
F1	0.9949	7.265	0.8566	0.345	0.8731	12.716	0.8798	0.031	0.9617	0.989
F2	0.9897	6.567	0.8966	0.189	0.9176	11.188	0.8583	0.022	0.9578	1.021
F3	0.9877	7.355	0.8898	0.278	0.9027	17.341	0.8865	0.043	0.9876	1.022
F4	0.9897	8.345	0.9045	0.176	0.8635	15.156	0.8758	0.021	0.9856	0.981
F5	0.9912	9.243	0.9256	0.177	0.8324	14.765	0.7898	0.027	0.9798	0.890
F6	0.9933	8.765	0.8763	0.156	0.8817	16.254	0.8495	0.031	0.9848	0.904
F7	0.9907	8.135	0.9374	0.099	0.8557	14.546	0.8145	0.023	0.9598	0.887
F8	0.9934	7.354	0.9532	0.343	0.8917	18.423	0.8732	0.021	0.9298	0.917
F9	0.9812	7.134	0.8684	0.423	0.9198	16.675	0.8912	0.032	0.9842	0.899
F10	0.9943	7.287	0.9067	0.257	0.9234	18.345	0.8548	0.024	0.9897	1.012
F11	0.9941	6.287	0.8994	0.232	0.9334	17.214	0.8267	0.018	0.9768	0.932
F12	0.9777	7.798	0.8190	0.231	0.8767	12.657	0.8187	0.029	0.9165	0.904
F13	0.9944	7.564	0.8588	0.199	0.8987	11.089	0.8756	0.024	0.9698	1.065
F14	0.9767	8.213	0.8744	0.324	0.8766	13.467	0.8498	0.034	0.9786	0.896
F15	0.9987	8.378	0.9143	0.213	0.9033	17.367	0.8576	0.025	0.9897	0.916
F16	0.9879	7.678	0.8878	0.254	0.8788	15.247	0.8687	0.032	0.9896	0.919
F17	0.9989	8.187	0.8033	0.222	0.8876	14.876	0.8997	0.037	0.9765	0.893
F18	0.9898	7.665	0.9189	0.167	0.8345	13.258	0.8898	0.019	0.9856	0.993
F19	0.9859	8.987	0.8978	0.213	0.8934	20.456	0.8667	0.034	0.9156	0.985
F20	0.9976	7.567	0.8788	0.213	0.8853	13.348	0.8745	0.028	0.9387	0.988



**Figure 3:** Thermograms and FTIR spectra. **A:** thermogram and FTIR spectrum of BW; **B:** thermogram and FTIR spectrum of nebivolol; **C:** thermogram and FTIR spectrum of nebivolol-loaded optimized LS



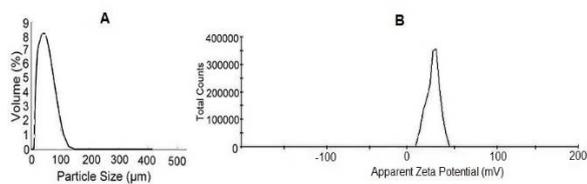
**Figure 4:** X-ray diffraction patterns of (a) BW, (b) nebivolol, and (c) nebivolol-loaded optimized LS



**Figure 5:** Scanning electron micrograph of OF

### Particle size and zeta potential

The size distribution of the LS ranged from 20 to 100  $\mu\text{m}$  (Figures 6A), while the major fraction (55 %) of LS had a mean size of 50  $\mu\text{m}$ . The zeta potential of OF was in the range of +15 to +35 mV (Figure 6B).



**Figure 6:** Particle size distribution and zeta potential curves. **A:** particle size distribution of OF; **B:** zeta potential curve of OF

## DISCUSSION

Hydrophilic and lipophilic drugs can be successfully delivered into deep and peripheral tissues by encapsulating them with crystalline lipids as LS. Lipospheres offer more advantages than the single-unit systems with respect to their uniform distribution in the gastrointestinal tract resulting in uniform absorption of the encapsulated drug [5]. The present study examined the formulation and characterization of nebivolol-loaded LS using BW as drug carrier. In this study, twenty micron-sized LS were produced. The results of DSC analysis and FTIR spectroscopy did not reveal absence or shift of any principal peaks of nebivolol and BW either in the spectrum of OF or individual spectra, and thermograms of nebivolol with BW. These results suggest compatibility of nebivolol and BW, and are in agreement with those previously reported [17].

The pattern of X-ray diffraction of OF revealed sharp and scattered peaks of nebivolol, an indication that nebivolol may have remained in crystalline form and that the process of formulation did not produce any negative effects on it [18]. The ratio of BW to surfactant strongly influenced rheology, morphology, PY, EE and size distribution of formulated LS. High concentrations of T-20 and SS contributed significantly to the production of free-flowing, smooth, spherical and micron-sized LSs [19].

These results are in agreement with those previously reported for lipid-based microparticles of somatostatin and oxybenzone [8,13]. The zeta potential of OF appears to suggest good stability since positive charge would naturally generate electrostatic repulsion between LSs, thereby preventing their aggregation [19]. It appears that increased concentrations of BW and T-20 are favorable conditions for producing high PY and EE, and that attainment of both requires concomitant increase in SS [17]. Low PY and EE may be associated with increased aggregation of lipids at low concentration of T-20, while high concentration of T-20 may prevent drug loss in

external phase and stabilization of lipid microparticles [17].

In this study, increased concentrations of BW, T-20, and SS resulted in increases in PY and EE (for  $Y_1$  and  $Y_2$ ). This suggests that BW, T-20 and SS may have positive impacts on PY and EE. For  $Y_1$ , the terms  $X_1$ ,  $X_2$ ,  $X_3$ , and  $X_1X_2$  were significant, an indication that BW, T-20, and SS may significantly affect PY [11]. The interaction of BW with T-20 ( $X_1X_2$ ) and T-20 with SS ( $X_2X_3$ ) were synergistic with respect to  $Y_1$  and  $Y_2$  [16]. High  $X_1$  negatively affected  $Y_3$ , an indication that an increase in BW concentration may retard drug release [18]. In addition, BW interaction with T-20 ( $X_1X_2$ ) produced sustained release nebigolol-loaded LS. However, the role of SS was critical. These results are in agreement with those previously reported [19]. The drug release followed a zero order model. It is possible that the underlying mechanism of drug release involves diffusion accompanied by erosion [3,19]. The selection of OF was made on attainment of maximum PY, maximum EE and minimum DR<sub>12</sub> [20].

## CONCLUSION

The results obtained in this study have shown that BW is a suitable material for producing a good sustained release formulation of nebigolol. The mechanism of drug release in nebigolol-loaded LS involves diffusion and erosion.

## DECLARATIONS

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### Conflict of Interest

No conflict of interest associated with this work.

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